Energy cost of walking and running at extreme uphill and downhill slopes

ALBERTO E. MINETTI,[2] CHRISTIAN MOIA,[1] GIULIO S. ROI,[3]
DAVIDE SUSTA,[1] AND GUIDO FERRETTI[1]
[1]*Département de Physiologie, Centre Médical Universitaire, 1211 Genève 4, Switzerland;* [2]*Centre for Biophysical and Clinical Research into Human Movement, Department of Exercise and Sport Science, Manchester Metropolitan University, Alsager, Cheshire ST7 2HL, United Kingdom; and* [3]*Medical Committee, Federation for Sport at Altitude, 13900 Biella, Italy*

Minetti, Alberto E., Christian Moia, Giulio S. Roi, Davide Susta, and Guido Ferretti. Energy cost of walking and running at extreme uphill and downhill slopes. *J Appl Physiol* 93: 1039–1046, 2002; 10.1152/japplphysiol. 01177.2001.—The costs of walking (Cw) and running (Cr) were measured on 10 runners on a treadmill inclined between −0.45 to +0.45 at different speeds. The minimum Cw was 1.64 ± 0.50 J·kg^{-1}·m^{-1} at a 1.0 ± 0.3 m/s speed on the level. It increased on positive slopes, attained 17.33 ± 1.11 J·kg^{-1}·m^{-1} at +0.45, and was reduced to 0.81 ± 0.37 J·kg^{-1}·m^{-1} at −0.10. At steeper slopes, it increased to reach 3.46 ± 0.95 J·kg^{-1}·m^{-1} at −0.45. Cr was 3.40 ± 0.24 J·kg^{-1}·m^{-1} on the level, independent of speed. It increased on positive slopes, attained 18.93 ± 1.74 J·kg^{-1}·m^{-1} at +0.45, and was reduced to 1.73 ± 0.36 J·kg^{-1}·m^{-1} at −0.20. At steeper slopes, it increased to reach 3.92 ± 0.81 J·kg^{-1}·m^{-1} at −0.45. The mechanical efficiencies of walking and running above +0.15 and below −0.15 attained those of concentric and eccentric muscular contraction, respectively. The optimum gradients for mountain paths approximated 0.20–0.30 for both gaits. Downhill, Cr was some 40% lower than reported in the literature for sedentary subjects. The estimated maximum running speeds on positive gradients corresponded to those adopted in uphill races; on negative gradients they were well above those attained in downhill competitions.

gradients; exercise; optimum path; maximum running speed

THE ENERGY COSTS OF LEVEL walking (Cw) and running (Cr) in humans have been extensively investigated (e.g., Refs. 4, 10, 12, 14, 15). Cw varies as a function of the speed, showing a minimum value at ~1.3 m/s. Cr is independent of the speed. Both Cw and Cr depend on the characteristics of the terrain, resulting higher on soft than on hard ground (13, 27). Adding a 1-kg load on the lower limbs increases Cr up to 7%, depending on where masses are added (16). Cr is also affected by the foot landing patterns, which allow a different efficiency of leg muscles and tendons (2) and increase when muscles are fatigued (5).

When walking or running on positive gradients, both the minimum Cw and the Cr increase as a function of the incline [up to +0.15 for running and up to +0.40 for walking (14, 15)]. When negative gradients are applied, both Cr and the minimum Cw attain their lowest value at −0.10. Below this slope, and down to −0.20 for running and to −0.40 for walking, minimum Cw and Cr are negatively related to the incline, becoming higher the lower the slope (14, 15). The range of running gradients (from −0.20 to +0.15), narrower than for walking, was set by the aerobic power of the subjects, none of whom was a professional long-distance runner.

Margaria (14) introduced also the concept of "mechanical efficiency," defined as the ratio of mechanical work for vertical displacement to the energy expended. He adopted the approximation of considering just the mechanical potential work (and disregarding the kinetic one) because he assumed that beyond a given gradient the rise (or descent) of the center of mass is the prevailing contributor to the mechanical external work. This assumption was supported by recent research (19, 20), which set the ±0.15 gradient as the threshold for pure positive and negative work in uphill and downhill locomotion, respectively. At slopes above +0.20, Margaria found that the efficiency of walking was ~0.25, i.e., close to that of concentric muscle contractions (26). At slopes below −0.20, the mechanical efficiency of walking was about −1.20, as for eccentric muscular contractions (1). Margaria postulated that this would have been the case also for running. Successively, little attention was paid to the study of the cost of locomotion at extreme slopes, despite the fact that in recent years walking and running on mountain paths became common practices in leisure time and sport. Davies et al. (8) studied one subject running downhill at −0.40; their results appear to agree with Margaria's hypothesis. To our knowledge, however, no systematic study of Cr during downhill and uphill running has been carried out so far.

The aim of the present study was to determine Cw and Cr on men walking and running on a treadmill at slopes ranging from -0.45 to $+0.45$, to encompass, especially for running, a wider range of slopes than in any previous study. In addition, we compared the maximum estimated running speeds as a function of the gradient, with the top performances in just-uphill and just-downhill fell running races.

METHODS

Subjects. After local ethical approval, 10 subjects were admitted to the study [men age 32.6 ± 7.5 yr, body mass 61.2 ± 5.7 kg, maximal O_2 consumption ($\dot{V}_{O_2 \, max}$) 68.9 ± 3.8 ml·min^{-1}·kg^{-1}]. They were all elite athletes practicing endurance mountain racing.

Methods. The O_2 consumption ($\dot{V}_{O_2}$) and CO_2 output ($\dot{V}_{CO_2}$) at rest and at the exercise steady state were measured by the standard open-circuit method. Expired air was collected in Douglas bags and analyzed for gas composition by use of O_2 and CO_2 analyzers (Leybold Haereus) and for volume by using a dry gas meter (Singer). $\dot{V}_{O_2}$ and $\dot{V}_{CO_2}$ were then calculated and expressed in STPD. $\dot{V}_{O_2 \, max}$ was measured by an incremental exercise test on the treadmill.

Heart rate was measured continuously by cardiotachography (Polar), and blood lactate concentration was determined after each run by an electroenzymatic method (Eppendorf EBIO 6666) on 20-μl micro blood samples from an ear lobe as a check for submaximal aerobic exercise.

The rate of metabolic energy expenditure (Ė, in W/kg) was calculated from the net $\dot{V}_{O_2}$ values (measured minus resting) assuming an energy equivalent of 20.9 kJ/l O_2 (corresponding to a nonproteic respiratory exchange ratio of 0.96). Cw and Cr were calculated (J·kg^{-1}·m^{-1}) as the ratio between Ė and the nominal speed. The mechanical efficiency of locomotion was calculated as the ratio of the mechanical work rate ($\dot{W}_{vert}$, W/kg) done to lift or absorbed in lowering the body mass at each stride to the rate of metabolic energy expenditure. $\dot{W}_{vert}$ was calculated as

$$\dot{W}_{vert} = gv \sin (\arctan |i|) \qquad (1)$$

where g is gravity acceleration (9.81 m/s^2), v is the treadmill speed (m/s), and i is the gradient.

Procedure. Each subject performed up to three walking and three running trials on a motor-driven treadmill at progressively increasing speeds on the level, and at the slopes of 0.10, 0.20, 0.30, 0.35, 0.40, and 0.45 uphill and downhill. Each trial lasted 4 min. Expired gas was collected into Douglas bag in the course of the fourth minute of exercise and analyzed immediately after the end of the trial. During uphill running, two consecutive trials were separated by 5-min recovery intervals, during which blood was taken for lactate determinations at *minutes 1, 3,* and *5.*

Before a test was performed, the speed of spontaneous transition between walking and running was identified empirically. Each test was performed according to an incremental procedure. At all gradients the speed of the first walking trial, carried out at the lowest investigated speed, was 0.69 m/s. The subsequent walking speeds were chosen in such a way as to stay within the speed range between 0.69 m/s and the apparent spontaneous transition speed. When possible, the speed increment was 0.42 m/s. The speed of the first running trial was set equal to the spontaneous transition speed. For the successive two trials at faster speeds, an increment of 0.56 m/s was usually imposed. This increment was reduced at high positive slopes, to cope with the need of

performing submaximal exercise trials. However, in some cases, a test was interrupted without completing the three running speeds, if blood lactate accumulation was higher than 4 mM. This happened particularly at the highest positive slopes, and on four subjects running could not be performed at slopes of $+0.40$ and $+0.45$.

RESULTS

$\dot{V}_{O_2}$ increased as a function of speed from 0.69 m/s onward during walking. During running, it increased linearly with the speed. At each speed, it was higher the higher the uphill gradient. The $\dot{V}_{O_2}$ values observed at the highest tested speed on the level and during uphill locomotion at each slope are reported in Table 1, together with the corresponding heart rate and blood lactate values.

The Cw on the level was 1.85 ± 0.57 J·kg^{-1}·m^{-1} at the speed of 0.69 m/s. The average minimum Cw was 1.64 ± 0.50 J·kg^{-1}·m^{-1} at a speed of 1.0 ± 0.3 m/s. The minimum Cw is plotted in Fig. 1*A* as a function of the slope. During uphill walking, the minimum Cw increased with the slope. At the slope of $+0.45$, minimum Cw was 17.33 ± 1.11 J·kg^{-1}·m^{-1} at the speed of 0.69 m/s for all subjects. During downhill walking, the minimum Cw attained its lowest value (0.81 ± 0.37 J·kg^{-1}·m^{-1}) at the slope of -0.10 at the average speed of 3.14 ± 0.22 m/s. At slopes below -0.10, it progressively increased. At -0.45, it was 3.46 ± 0.95 J·kg^{-1}·m^{-1}.

Cr on the level was 3.40 ± 0.24 J·kg^{-1}·m^{-1}, independent of speed. The average Cr at the investigated speeds is plotted in Fig. 1*B* as a function of the slope. Cr increased with the slope uphill to attain 18.93 ± 1.74 J·kg^{-1}·m^{-1} at $+0.45$. This value was only $9.2 \pm 2.6\%$ higher than the minimum Cw at the same slope, whereas on the level Cr was $107.3 \pm 49.8\%$ higher than the minimum Cw. During downhill running, Cr decreased and attained its lowest value at -0.20 (1.73 ± 0.36 J·kg^{-1}·m^{-1}). At lower slopes it increased again. At -0.45, it was 3.92 ± 0.81 J·kg^{-1}·m^{-1}. The average minimum Cw and the Cr observed at each investigated slopes are summarized in Table 2.

Table 1. *Metabolic parameters of running at the highest tested speed at each uphill slope*

Slope	Speed, m/s	$\dot{V}_{O_2}$, ml·kg^{-1}·min^{-1}	Heart Rate, min^{-1}	Lactate, mM
−0.45	1.63 ± 0.40	23.2 ± 3.3	131 ± 36	
−0.40	1.86 ± 0.30	23.5 ± 2.3	122 ± 26	
−0.35	2.14 ± 0.22	22.2 ± 3.0	116 ± 23	
−0.30	2.52 ± 0.58	22.0 ± 3.1	113 ± 17	
−0.20	2.84 ± 0.39	18.9 ± 2.6	100 ± 13	
−0.10	3.08 ± 0.26	23.3 ± 5.7	101 ± 8	
0.00	3.13 ± 0.22	35.5 ± 2.7	125 ± 15	2.30 ± 0.73
0.10	2.90 ± 0.27	53.0 ± 8.6	158 ± 11	3.05 ± 1.17
0.20	2.11 ± 0.27	56.2 ± 4.4	168 ± 13	3.20 ± 0.81
0.30	1.46 ± 0.12	58.4 ± 2.9	169 ± 10	3.47 ± 0.77
0.35	1.18 ± 0.14	57.5 ± 2.6	167 ± 12	3.18 ± 0.65
0.40	0.99 ± 0.10	55.5 ± 1.2	169 ± 15	3.18 ± 0.18
0.45	0.89 ± 0.10	52.1 ± 4.2	167 ± 14	3.16 ± 0.46

Values are means $\pm$ SD. $\dot{V}_{O_2}$ is the overall steady-state oxygen consumption.
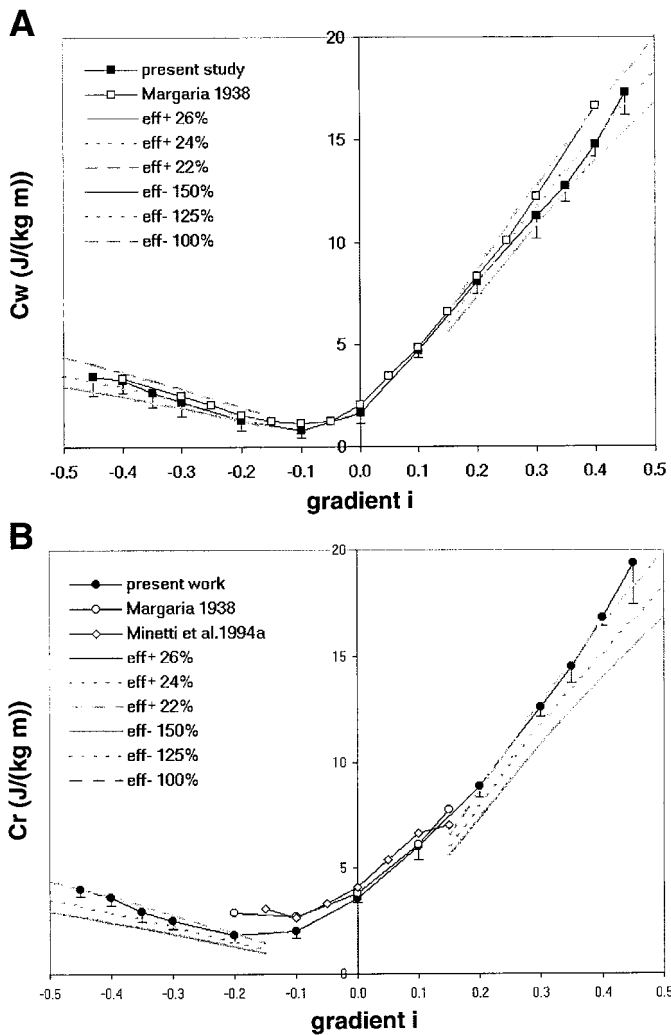
Fig. 1. Metabolic energy cost of walking (Cw; *A*) or running (Cr; *B*) as a function of the gradient from the present investigation and from the work by Margaria (14, 15) and Minetti et al. (20, only for running). Minimum energy cost of walking and average energy cost of running for each gradient have been reported. To accurately describe the relationship between Cw or Cr and the gradient *i* within the investigated range, 5th-order polynomial regressions were performed, that yielded

$$\text{Cw}_i = 280.5i^5 - 58.7i^4 - 76.8i^3 + 51.9i^2 + 19.6i + 2.5 \quad (R^2 = 0.999)$$

$$\text{Cr}_i = 155.4i^5 - 30.4i^4 - 43.3i^3 + 46.3i^2 + 19.5i + 3.6 \quad (R^2 = 0.999)$$

Gray curves represent the metabolic cost corresponding to a given positive and negative efficiency, according to

$$C_{eff} = \frac{\dot{W}_{vert}}{v \; eff} = \frac{g \, \sin \, (\text{arc tan } |i|)}{eff}$$

where C is metabolic cost, $\dot{W}_{vert}$ is vertical work rate, v is treadmill speed, g is gravity acceleration, and eff is efficiency. The eff values for uphill and downhill locomotion, respectively, were chosen as equal to 26% and 150% (solid curve), 24% and 125% (finely dashed curve), and 22% and 100% (grossly dashed curve).

The vertical cost of walking and running ($J \cdot kg^{-1} \cdot m_{vert}^{-1}$) is defined as the energy expenditure to walk or to run a distance that corresponds to a vertical displacement of 1 m. It is plotted in Fig. 2*A* for walking and in Fig. 2*B* for running. The vertical cost decreased during uphill running to attain a minimum value of 44.9 ± 3.8

$J \cdot kg^{-1} \cdot m^{-1}$ in the slope range of 0.20–0.40. During downhill running, the vertical cost decreased, to attain a minimum of 9.2 ± 1.7 $J \cdot kg^{-1} \cdot m^{-1}$ in the slope range from −0.20 to −0.40.

The mechanical efficiency for running is shown in Fig. 3. For uphill slopes steeper than +0.15, they were 0.243 ± 0.012 and 0.218 ± 0.06 for walking and running, respectively. For downhill slopes steeper than −0.15, they were −1.215 ± 0.184 and −1.062 ± 0.056, respectively.

DISCUSSION

The present study demonstrates that uphill Cw and Cr data are directly proportional to the slope above +0.15, compatibly with a mechanical efficiency of 0.22–0.24. During downhill locomotion, Cw and Cr show a linear negative relation with the slope below −0.15, compatibly with a mechanical efficiency of −1.06 to −1.21. These results fully support the hypothesis of Margaria and co-workers (14, 15), according to which the efficiency of uphill locomotion at sufficiently high slopes ought to become equal to that of concentric muscular work, whereas downhill efficiency ought to become close to that of negative work, i.e., −1.2 (1). It is important to remember that the mechanical efficiency mentioned so far is calculated by dividing the potential energy changes by the metabolic consumption; thus those values are reliable only when the kinetic energy changes are incomparably smaller and when only positive or only negative work is associated to the motion of the body center of mass. In Fig. 3, the arrow defines the gradient range ±0.15, within which the mechanical external work of walking (19) and running (20) is still contributed by a mixture of positive and negative work. For steeper positive gradients, the 0.25 efficiency value implies that all the work be done to lift the body: only positive work is done in both gaits, and the descending phase of the pendulum-like and bouncing ball (6) mechanisms of walking and running is lost. By analogy, for steeper negative gradients, the −1.2 efficiency value implies that only negative work is done in both gaits and that the ascending phase of the pendulum-like and bouncing ball (6) mechanisms of walking and running is lost. Because either mechanism requires both an ascending and a descending phase of the trajectory to allow for the recovery of mechanical energy, the concept (21) that walking and running, when operated at gradients steeper than the ±0.15 range, lose the pendulum-like and the bouncing-ball mechanism, respectively, is reinforced. If this is so, and if we consider how Cw and Cr become close at the steepest gradients, we wonder whether it is legitimate to speak of "walking" or "running" at the steepest slopes. A biomechanical study of walking and running on steep gradient would be required for an appropriate characterization of the gait and for a clear identification, from the measure of contact times, of the transition from a walkinglike to a runninglike gait when the differences between walking and running tend to disappear.

Table 2. *Minimum cost of walking and cost of running at the indicated slopes on the treadmill*

Slope	Cw	Cr	Slope	Cw	Cr	Slope	Cw	Cr
−0.45	$n = 10$	$n = 9$	0	$n = 10$	$n = 30$	0.45	$n = 10$	$n = 6$
	3.46 ± 0.95	3.92 ± 0.81		1.64 ± 0.50	3.40 ± 0.24		17.33 ± 1.11	18.93 ± 1.74
−0.40	$n = 10$	$n = 13$				0.40	$n = 10$	$n = 6$
	3.23 ± 0.59	3.49 ± 0.47					14.75 ± 0.61	16.83 ± 0.88
−0.35	$n = 10$	$n = 18$				0.35	$n = 10$	$n = 12$
	2.65 ± 0.68	2.81 ± 0.54					12.72 ± 0.76	14.43 ± 1.08
−0.30	$n = 10$	$n = 24$				0.30	$n = 10$	$n = 24$
	2.18 ± 0.67	2.43 ± 0.50					11.29 ± 1.14	12.52 ± 0.62
−0.20	$n = 10$	$n = 24$				0.20	$n = 10$	$n = 30$
	1.30 ± 0.48	1.73 ± 0.36					8.07 ± 0.57	8.92 ± 0.84
−0.10	$n = 10$	$n = 24$				0.10	$n = 10$	$n = 30$
	0.81 ± 0.37	1.93 ± 0.45					4.68 ± 0.34	5.77 ± 0.60

Values are means ± SD. Cw, cost of walking; Cr, cost of running.

A comparison of the present results with those from previous studies is attempted in all the illustrated figures. Despite of the different methodology involved, the spontaneous speed of transition between walking and running is similar to the one reported in a subset of gradients (21). Although Cw is very similar to what previously reported (14), as shown in Fig. 1*A*, Cr seems to resemble the reported data (14, 15, 20) only at level and uphill gradients (see Fig. 1*B*). This suggests that the athletes presently investigated, specifically trained in fell-running, developed a more economical style than nonathletic subjects during descent. Because little can be done on the path of the center of mass at extreme slopes that could reduce the overall mechanical work, a possible explanation of the greater economy could be the decrease in cocontractions needed to stabilize the descent.

The vertical cost of walking and running on slopes has been introduced (18) to focus on the optimization of
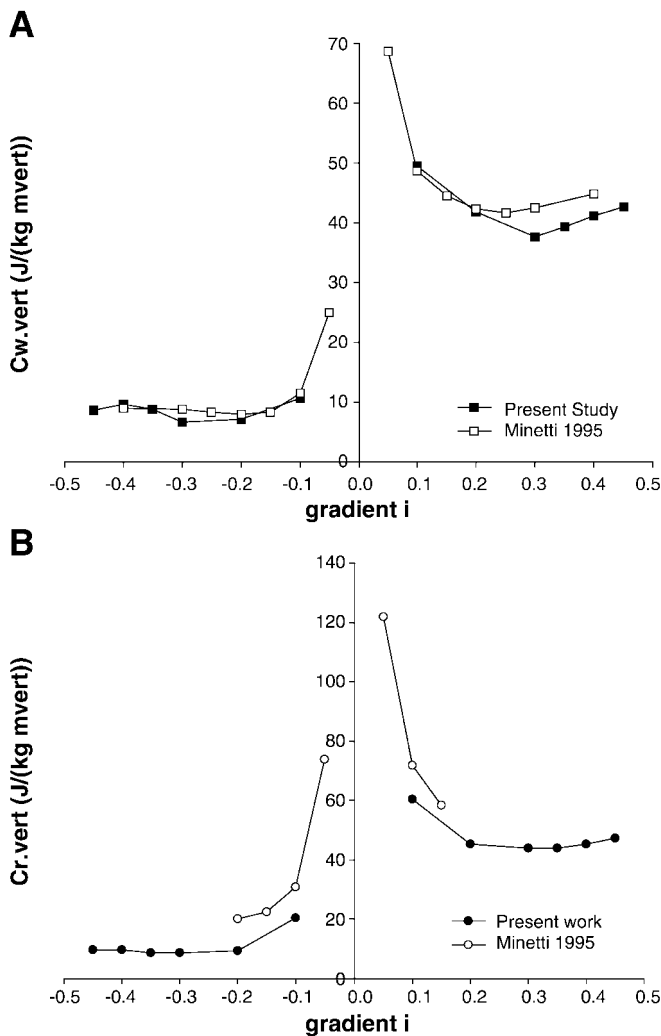

Fig. 2. Metabolic energy cost of walking (*A*) or running (*B*), expressed per unit of vertical distance (m$_{vert}$) as a function of the gradient, from the present investigation (■), and from Minetti (18), where reprocessed data from Margaria (14, 15) were presented.
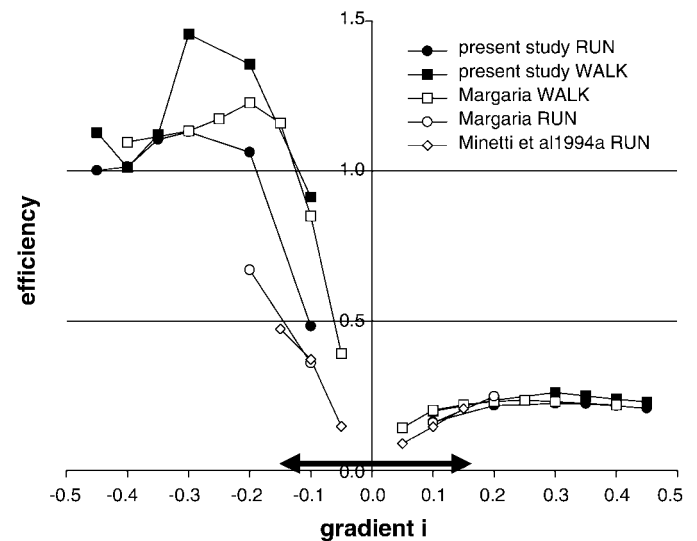

Fig. 3. Mechanical efficiency of the work done for the vertical displacement of the body during locomotion as a function of the gradient. Data are from the present investigation, from Margaria (14, 15) and from Minetti (20). Double-headed arrow parallel to the *x*-axis defines the gradient range where the external work of locomotion is contributed by a combination of positive and negative work. Note that the *y*-axis scale reports the absolute value of efficiency: the sign ought to be negative for downhill locomotion, positive for uphill locomotion.

mountain paths. It was concluded that for walking the gradient minimizing the metabolic cost should be $\sim$0.25–0.28, both uphill and downhill. This concept is essentially supported by the present results (see Fig. 2*A*), though the minimum vertical cost for downhill walking looks broader than expected. In running, it was previously impossible to estimate such an optimum gradient, mainly because of the limited slope range available (see Fig. 2*B*, open circles). The present work, by extending the slope range to $\pm$0.45, shows that it is similar to the one for walking, despite the broader minima: these probably reflect the athletes' ability to perform in very different conditions (see Fig. 2*B*). Particularly at downhill gradients, at which athletes report a 30–50% reduction in the vertical cost, a better technique allowing a greater recovery of elastic energy could be responsible for the increased economy.

From the results of the present investigation, it is now possible *1*) to estimate the maximum (aerobic) running speed as a function of both positive and negative gradient and *2*) to compare it with the best results from uphill-only and downhill-only races, available from official mountain Federation of Sport at Altitude competitions.

As indicated in METHODS, the metabolic energy cost ($Cr_{v,i}$, in $J\cdot kg^{-1}\cdot m^{-1}$) of running a unit distance at any given speed and gradient has been calculated as

$$Cr_{v,i} = \frac{\dot{E}_{v,i}}{v_i} \qquad (2)$$

where $\dot{E}_{v,i}$ is the net metabolic power (W/kg) measured during the experiments. It is widely known, and it was confirmed by this study too, that $Cr_{v,i}$ changes at each gradient *i* (see Fig. 2), but it is quite constant at all running speeds within every single gradient; thus the index *v* can be removed from that symbol. Such a peculiar characteristic of running, so different from
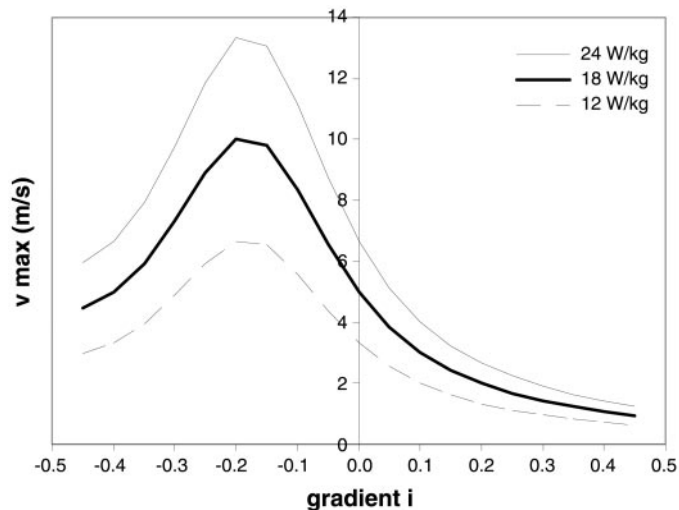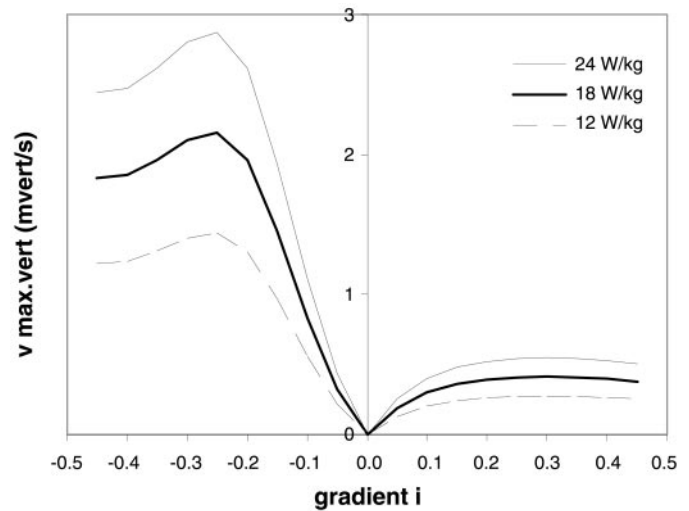

Fig. 5. Maximum running speed, expressed in vertical meters per second, vs. gradient, as predicted by combining *Eqs*. 2 and 3. The three curves refer to different $\dot{V}O_{2\,submax}$ values (net metabolic powers of 12, 18, and 24 W/kg).

other gaits such as walking, allows estimation at each gradient of the maximum running speed ($v_{max,i}$, m/s). The previous equation can be expressed as

$$v_{max,i} = \frac{\dot{E}_{max,i}}{Cr_i} \qquad (3)$$

where $\dot{E}_{max,i}$ is the maximum oxygen consumption (in W/kg) of the subjects group (11). Because only a fraction of the maximum metabolic power ($\dot{E}_{sub\,max,i}$) can be used to sustain aerobic exercise in long-lasting events (see below), and this last parameter is obviously independent from *i*, the last equation becomes

$$v_{max,i} = \frac{\dot{E}_{sub\,max}}{Cr_i} \qquad (4)$$

Once the numerator in *Eq. 2* has been set, say 18 W/kg, the maximum running speed is obtained, as shown by the thick curve in Fig. 4. Those estimates linearly scale with the maximum aerobic power or its sustainable fraction, as indicated by the other two curves in Fig. 4. The same applies to the calculation of the maximum vertical speed of running ($v_{max\,vert}$, m_{vert}/s), as obtained from

$$v_{max\,vert,i} = v_{max,i}\,\sin(arc\,\tan|i|) \qquad (5)$$

and shown in Fig. 5 for three levels of available metabolic power. For instance, $v_{max\,vert}$ was estimated to be $\sim$2.1 and 0.4 m_{vert}/s for downhill ($i = -0.25$) and uphill ($i = +0.25$) gradients, respectively, for a $\dot{V}O_{2\,submit}$ equal to 18 W/kg.

To compare these estimates to the real running speeds, as observed during competition, we could not expect the race results to follow a single curve in Fig. 4 or 5, because, even assuming that all the athletes report the same maximum aerobic power, two other main variables affect the available metabolic power during the event, even for the same average gradient.

Fig. 4. Maximum running speed on the incline, as a function of the gradient, as predicted by combining *Eqs. 2* and *3*. The 3 curves refer to different submaximal oxygen consumption ($\dot{V}O_{2\,submax}$) values (net metabolic powers of 12, 18 and 24 W/kg).

Table 3. *Predicted versus actual performances during uphill and downhill competitions*

Location, vertical km	Distance, km	Duration, s	Height, m	Altitude, m	Gradient	V_{vert} Measured, m_{vert}/s	Predicted, m_{vert}/s	Predicted/ Measured	$\dot{V}_{O_2}$ Predicted, $ml \cdot kg^{-1} \cdot min^{-1}$
					Up				
	2.9	2,132	981		0.360	0.460	0.407	0.884	62.4
Mt. Cameroon up	18.0	12,600	3,400	4,095	0.192	0.270	0.330	1.225	39.7
Mt. Washington	12.2	3,500	1417		0.117	0.405	0.318	0.786	68.1
Mt. Tennant	6.6	2,198	700		0.107	0.318	0.312	0.980	56.7
Mt. Ainslie	2.2	620	230		0.105	0.371	0.319	0.859	65.8
Cervinia vkm	3.5	2,544	1,000		0.298	0.393	0.409	1.042	53.2
Dolomites	10.0	5,004	1,702		0.173	0.340	0.359	1.056	50.3
Japan 1	15.0	4,633	1,480		0.099	0.319	0.287	0.898	58.8
Japan 2	21.0	9,383	3,000		0.144	0.320	0.309	0.967	50.3
Mean ± SD								0.950 ± 0.130	56.1 ± 8.9
					Down				
Kinabalu down	10.0	3,420	−2,205	4,095	−0.226	0.645	3.250	5.041	19.6
Pike's Peak	21.0	4,500	−2,200	4,301	−0.105	0.489	1.758	3.596	31.7
Breithorn	13.0	2,280	−2,160	4,165	−0.168	0.947	1.785	1.884	32.7
Mt. Blanc	16.0	5,520	−3,807	4,810	−0.245	0.690	3.001	4.351	20.3
Mt. Cameroon down	18.0	3,717	−3,400	4,095	−0.192	0.915	2.157	2.358	28.4
Mean ± SD								3.446 ± 1.324	26.5 ± 6.2

The assumption of a maximal rate of aerobic energy expenditure of 22.6 W/kg was made.

In fact, it is known that the available fraction of $\dot{V}_{O_2 max}$ ($\dot{E}_{max,i}$) depends on the exercise duration ($fract_{duration}$) (23) and on the altitude above sea level ($fract_{altitude}$) (7) at which the exercise is performed, and both effects are strongly involved in gradient running events. Thus we could write

$$\dot{E}_{sub\,max} = \dot{E}_{max}\,fract_{duration}\,fract_{altitude} \qquad (6)$$

where

$$fract_{duration} = \frac{940 - \dfrac{t_{event}}{60}}{1{,}000} \qquad (7)$$

adapted from Saltin (24), where t_{event} is the event duration, and

$$fract_{altitude} = 1 - 11.7 \cdot 10^{-9}altitude^2$$
$$- 4.01 \cdot 10^{-6}altitude \qquad (8)$$

from Cerretelli (7). In *Eqs. 7* and *8*, t_{event} and altitude are expressed in seconds and meters, respectively.

Table 3 reports data available from the Internet about some only-uphill and only-downhill running races. When the event best time, the distance traveled, the difference in altitude and, sometimes, the maximum altitude reached are known, the average gradient and the predicted $v_{max,i}$ and $v_{max\,vert}$ can be calculated by using *Eqs. 3-8*. In the sample of events shown in the table, the striking result is the very close match between predicted and measured maximum vertical speed in uphill running (their ratio is 0.950 ± 0.130), whereas predicted speed for downhill races overestimates the measured one by a factor of 3 (their ratio is 3.446 ± 1.324), as shown in Fig. 6.

Such a discrepancy is astonishingly too large to be explained in terms of differences in muscular efficiency only. In downhill competitions, athletes do not seem to use the full amount of the available aerobic power for increasing their speed. The reasons should be methodological and/or inherent in reproducing an outdoor condition in the laboratory. In the following, a list of potential determinants of such a speed choice is re-
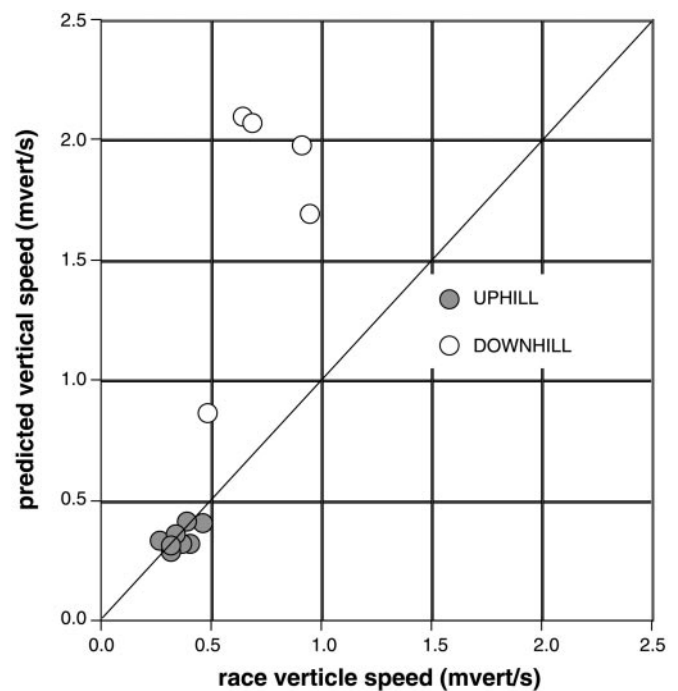

Fig. 6. Predicted maximum vertical speed vs. actual vertical speed as reported from mountain-running competitions. Predictions were made according to *Eqs. 3–8* and the data regarding distance, duration, and average altitude. Only uphill (gray circles) and only downhill (○) competitions are reported. The assumption of a maximal rate of aerobic energy expenditure of 22.6 W/kg was made.

ported in descending order for relevance (and likelihood).

1) During downhill running, other criteria such as the maintenance of a reasonable safety factor could be operating to minimize joint and tissue injuries. It is likely that at extreme downhill slopes muscles could not cope with the tendency of the body to accelerate, rather than maintaining a constant speed throughout a controlled constant braking. That would result in the lack of the fine motor control needed to maintain body trajectory on a rough and slippery terrain. Among the associated risks is the iliotibial band friction syndrome, more frequent in downhill running because the knee flexion angle at foot strike is reduced (22, 23), and the intravascular hemolysis due to foot impact forces (17) is high.

2) Methodological issues could have led *a*) to underestimation of Cr because of the differences in terms of path geometry and surface properties between the rough terrain and the smooth treadmill surface, a discrepancy particularly accentuated for downhill gradients because of the much higher speeds involved; and *b*) to overestimation of $v_{max,i}$ (and $v_{max \, vert}$) because the prediction for each gradient has been made outside the investigated speed range (extrapolation) by assuming Cr speed independent.

3) It has also been reported that, particularly in downhill running, *a*) a stricter alignment of locomotor-respiratory coupling occurs (25), which could be disrupted by even a slight increase in speed and related stride frequency; *b*) the motoneuron pool excitability decreases (3), with effects on the overall motor control; and *c*) a time-dependent upward drift of $\dot{V}O_2$ (+10%, which should proportionally increase Cr), and increase in EMG activity (9) take place.

This analysis points out how in competitive downhill running, differently from the uphill situation and many other sport activities, "power without control is nothing." To verify the relative contribution and the relevance of the hypothesized list of determinants for choosing to run slower than metabolically possible at extreme downhill gradients, further experiments on the capacity of the neuromusculoskeletal system to brake the body motion are needed.

In conclusion, the present study extends the previous literature about the economy of locomotion to include extreme slopes up to ± 0.45, an unprecedented range particularly for running. The results show that *1*) the minimum in energy cost is similar in walking and running at ~0.10–0.20 downhill gradient; *2*) the optimum gradient for mountain paths is close to 0.20–0.30, both uphill and downhill, for the two gaits; *3*) a better progression economy is expected in mountain-running athletes in the downhill range; and *4*) the running speeds adopted in downhill competition are far lower than metabolically feasible, mainly because of safety reasons. If athletes wish to improve their performances in competitions alternating ascent and descent phases, they should pay greatest attention to the training of movement coordination during downhill running.

REFERENCES

1. **Abbott B, Bigland B, and Ritchie JM.** The physiological cost of negative work. *J Physiol* 117: 380–390, 1952.
2. **Ardigò LP, Lafortuna C, Minetti AE, Mognoni P, and Saibene F.** Metabolic and mechanical aspects of foot landing type, forefoot and rearfoot strike, in human running. *Acta Physiol Scand* 155: 17–22, 1995.
3. **Bulbulian R and Bowles DK.** Effect of downhill running on motoneuron pool excitability. *J Appl Physiol* 73: 968–973, 1992.
4. **Bobbert AC.** Energy expenditure in level and grade walking. *J Appl Physiol* 15: 1015–1021, 1960.
5. **Brueckner JC, Atchou G, Capelli C, Duvallet A, Barrault D, Jousselin E, Rieu M, and di Prampero PE.** The energy cost of running increases with the distance covered. *Eur J Appl Physiol* 62: 385–389, 1991.
6. **Cavagna GA, Thys H, and Zamboni A.** The sources of external work in level walking and running. *J Physiol* 262: 639–657, 1976.
7. **Cerretelli P.** Limiting factors to oxygen transport on Mount Everest. *J Appl Physiol* 40: 658–667, 1976.
8. **Davies CTM, Sargeant AJ, and Smith B.** The physiological responses to running downhill. *Eur J Appl Physiol* 32: 187–194, 1974.
9. **Dick RW and Cavanagh PR.** An explanation of the upward drift in oxygen uptake during prolonged sub-maximal downhill running. *Med Sci Sports Exerc* 19: 310–317, 1987.
10. **Di Prampero PE.** The energy cost of human locomotion on land and in water. *Int J Sports Med* 7: 55–72, 1986.
11. **Di Prampero PE, Atchou G, Brückner JC, and Moia C.** The energetics of endurance running. *Eur J Appl Physiol* 55: 259–266, 1986.
12. **Dill DB.** Oxygen used in horizontal and grade walking and running on the treadmill. *J Appl Physiol* 20: 19–22, 1965.
13. **Lejeune TM, Willems PA, and Heglund NC.** Mechanics and energetics of human locomotion on sand. *J Exp Biol* 201: 2071–2080, 1998.
14. **Margaria R.** Sulla fisiologia e specialmente sul consumo energetico della marcia e della corsa a varia velocità ed inclinazione del terreno. *Atti Accademia Nazionale dei Lincei* 7: 299–368, 1938.
15. **Margaria R, Cerretelli P, Aghemo P, and Sassi G.** Energy cost of running. *J Appl Physiol* 18: 367–370, 1963.
16. **Martin PE.** Mechanical and physiological responses to lower extremity loading during running. *Med Sci Sports Exerc* 17: 427–433, 1985.
17. **Miller BJ, Pate RR, and Burgess W.** Foot impact force and intravascular hemolysis during distance running. *Int J Sports Med* 9: 56–60, 1988.
18. **Minetti AE.** Optimum gradient of mountain paths. *J Appl Physiol* 79: 1698–1703, 1995.
19. **Minetti AE, Ardigò LP, and Saibene F.** Mechanical determinants of gradient walking energetics in man. *J Physiol* 471, 725–735, 1993.
20. **Minetti AE, Ardigò LP, and Saibene F.** Mechanical determinants of the minimum energy cost of gradient running in humans. *J Exp Biol* 195, 211–225, 1994.
21. **Minetti AE, Ardigò LP, and Saibene F.** The transition between walking and running in man: metabolic and mechanical aspects at different grades. *Acta Physiol Scand* 150: 315–323, 1994.
22. **Noble CA.** Iliotibial band friction syndrome in runners. *Am J Sports Med* 8: 232–234, 1980.
23. **Orchard JW, Fricker PA, Abud AT, and Mason BR.** Biomechanics of iliotibial band friction syndrome in runners. *Am J Sports Med* 24: 375–379, 1996.

24. **Saltin B.** Oxygen transport by the circulatory system during exercise in man. In: *Limiting Factors of Physical Performance*, edited by Keul J. Stuttgart: Thieme, 1973, p. 235–252.

25. **Takano N.** Phase relation and breathing pattern during locomotor/respiratory coupling in uphill and downhill running. *Jpn J Physiol* 45: 47–58, 1995.

26. **Woledge RC, Curtin NA, and Homsher E.** *Energetic Aspects of Muscle Contraction*. London: Academic, 1985, p. 267. (Monographs of the Physiological Society 41)

27. **Zamparo P, Perini R, Orizio C, Sacher M, and Ferretti G.** The energy cost of walking or running on sand. *Eur J Appl Physiol* 65: 183–187, 1992.